

# FINITE ELEMENT ANALYSIS FOR BIOMEDICAL ENGINEERING APPLICATIONS

Z. Yang



## Finite Element Analysis for Biomedical Engineering Applications



# Finite Element Analysis for Biomedical Engineering Applications

Z. Yang



CRC Press Taylor & Francis Group 6000 Broken Sound Parkway NW, Suite 300 Boca Raton, FL 33487-2742

© 2019 by Taylor & Francis Group, LLC CRC Press is an imprint of Taylor & Francis Group, an Informa business

No claim to original U.S. Government works

Printed on acid-free paper

International Standard Book Number-13: 978-0-367-18218-2 (Hardback)

This book contains information obtained from authentic and highly regarded sources. Reasonable efforts have been made to publish reliable data and information, but the author and publisher cannot assume responsibility for the validity of all materials or the consequences of their use. The authors and publishers have attempted to trace the copyright holders of all material reproduced in this publication and apologize to copyright holders if permission to publish in this form has not been obtained. If any copyright material has not been acknowledged please write and let us know so we may rectify in any future reprint.

Except as permitted under U.S. Copyright Law, no part of this book may be reprinted, reproduced, transmitted, or utilized in any form by any electronic, mechanical, or other means, now known or hereafter invented, including photocopying, microfilming, and recording, or in any information storage or retrieval system, without written permission from the publishers.

For permission to photocopy or use material electronically from this work, please access <a href="www.copyright.com">www.copyright.com</a> (Mttp://www.copyright.com</a>) or contact the Copyright Clearance Center, Inc. (CCC), 222 Rosewood Drive, Danvers, MA 01923, 978-750-8400. CCC is a not-for-profit organization that provides licenses and registration for a variety of users. For organizations that have been granted a photocopy license by the CCC, a separate system of payment has been arranged.

**Trademark Notice:** Product or corporate names may be trademarks or registered trademarks, and are used only for identification and explanation without intent to infringe.

Visit the Taylor & Francis Web site at http://www.taylorandfrancis.com and the CRC Press Web site at http://www.crcpress.com

### Contents

Chapter 1	Intro	duction.			1			
PART I	Bor	1e						
Chapter 2	Bone	Bone Structure and Material Properties						
	2.1 2.2 Refe	Materi	al Properti	es of Bone	7			
Chapter 3	Simu	ılation of	Nonhomo	geneous Bone	9			
	3.1	3.1.1 3.1.2 3.1.3 3.1.4 3.1.5	CT Data Finite El Calculat Material Discussi	lodel from CT Data	. 10 . 10 . 10 . 13 . 14			
	3.2	3.1.6 Interpo		y  Bone Material Properties				
	3 <b>.2</b>	3.2.1		nensional Interpolation  RBAS Algorithm  NNEI Algorithm  LMUL Algorithm	. 15 . 15 . 15			
		3.2.2		ation of Material Properties of le	. 16			
			3.2.2.2	Bone Using the RBAS Algorithm Defining Material Properties of				
			3.2.2.3	Bone Using the NNEI Algorithm Defining Material Properties of Bone Using the LMUL Algorithm				
			3.2.2.4	Defining Material Properties of Bone Using a Mixed Method	. 19			
		3.2.3 3.2.4	Summar	ony	. 20 . 21			
	Refe	rences			. 21			

vi Contents

Chapter 4	Simu	ılation of	Anisotropic Bone	23		
	4.1 4.2	Finite I	ropic Material Models Element Model of Femur with Anisotropic als			
		4.2.1	Finite Element Model of Femur with			
			Anisotropic Materials			
		4.2.2	Simulation of Mechanical Testing of the Femur			
		4.2.3				
	D C	4.2.4	·- · · · · · · · · · · · · · · · · ·			
	Refe	rences		31		
Chapter 5			Crack Growth Using the eXtended Finite and (XFEM)	22		
	Licii					
	5.1		ection to XFEM	33		
		5.1.1	Singularity-Based Method			
		5.1.2	Phantom-Node Method	34		
		5.1.3	General Process for Performing XFEM			
	<i>-</i>	G: 1	Crack-Growth Simulation			
	5.2		tion of Crack Growth of the Cortical Bone			
		5.2.1	Finite Element Model			
			5.2.1.1 Geometry and Mesh			
			5.2.1.2 Material Properties			
			5.2.1.4 Local Coordinate Systems			
			5.2.1.5 Loading and Boundary Conditions			
			5.2.1.6 Solution Setting			
		5.2.2	Results			
		5.2.3				
		5.2.4				
	Refe					
		a•				
PART II	So	tt Tissi	ues			
Chapter 6	Struc	Structure and Material Properties of Soft Tissues				
	6.1		ge			
		6.1.1	Structure of Cartilage			
		6.1.2	Material Properties of Cartilage			
	6.2	_	ents			
		6.2.1	Structure of Ligaments			
	( )	6.2.2	Material Properties of Ligaments			
	6.3		rtebral Disc	47 48		
	References 4					

Contents

Chapter 7	Nonlinear Behavior of Soft Tissues				
	7.1 7.2	Finite 1	Element Ai	lelsnalysis of the Abdominal Aortic	
		7.2.1		ement Model	
			7.2.1.1	Geometry and Mesh	
			7.2.1.2	Material Model	
			7.2.1.3	Loading and Boundary Conditions	
		7.2.2	7.2.1.4	Solution Setting	
		7.2.2			
		7.2.3		on	
	D . C.	7.2.4		y	
	rece				50
Chapter 8	Visc	oelasticit	y of Soft T	issues	61
	8.1	The M	axwell Mo	del	61
	8.2	Study of	of PDL Cre	eep	63
		8.2.1	Finite Ele	ement Model	63
			8.2.1.1	Geometry and Mesh	63
			8.2.1.2	Material Models	64
			8.2.1.3	Boundary Conditions	64
			8.2.1.4	Loading Steps	65
		8.2.2	Results .		65
		8.2.3	Discussion	on	65
		8.2.4	Summary	y	67
	Refe	rences			67
Chapter 9	Fiber	r Enhance	ement		69
Chapter					
	9.1	Standa 9.1.1		nhancementtion of Standard Fiber	69
			Enhancer	ment	69
		9.1.2	IVD Mod	del with Fiber Enhancement	69
			9.1.2.1	Finite Element Model of IVD	70
			9.1.2.2	Results	73
			9.1.2.3	Discussion	73
			9.1.2.4	Summary	75
	9.2	Mesh-I	ndependen	nt Fiber Enhancement	75
		9.2.1	_	tion of Mesh-Independent Fiber	
				ment	75
		9.2.2	IVD Mod	del with Mesh-Independent Fiber	
			Enhancer	ment	76
			9221	Finite Element Model	76

viii Contents

			9.2.2.2	Creating the Fibers	76
			9.2.2.3	Results	78
			9.2.2.4	Summary	79
	9.3	Material	Models I	ncluding Fiber Enhancement	79
				oic Material Model with Fiber	
			Enhancer	nent	79
		9.3.2	Simulatio	on of Anterior Cruciate	
			Ligament	: (ACL)	84
			9.3.2.1	Finite Element Model	85
			9.3.2.2	Results	88
			9.3.2.3	Discussion	88
			9.3.2.4	Summary	88
	Refere	ences			90
Chapter 10	USER	RMAT for	Simulation	on of Soft Tissues	93
•	10.1	T., 4.,	-4:£ C	behanding Hondless	0.2
	10.1			Subroutine UserHyper	
	10.2			AA Using UserHyper	93
		10.2.1		Subroutine UserHyper to Simulate	0.2
		10.2.2		ssues of the Artery	
		10.2.2		tion	
		10.2.3	-	the AAA Using UserHyper	
		10.2.4		sion	
	D.C	10.2.5		ary	
	Refere	ences	• • • • • • • • •		99
Chapter 11	Mode	ling Soft	Tissues as	s Porous Media	101
	11.1	CPT EI	ements		101
	11.2			mpact	
	11.2	11.2.1		Element Model of the Head	
		11.2.1	11.2.1.		
			11.2.1.	•	
			11.2.1.	-	102
			11.2.1.	Conditions	102
		11.2.2	Results	S	
		11.2.3		sion	
		11.2.4		ary	
	11.3			eep Behavior of the IVD	
	11.5	11.3.1		Element Method	
		11.3.1	11.3.1.		
			11.3.1.	· ·	
			11.3.1.	-	100
			11.3.1.	Conditions	100
			11 3 1		109
			1131	→ ,1011111011 ,15111110	1119

Contents ix

		11.3.2	Results		110	
		11.3.3	Discussion	1	111	
		11.3.4	•			
	Refere	ences	•••••		113	
PART III	Join	ts				
Chapter 12	Struct	ure and Fu	unction of Jo	ints	117	
	Refere	ence			118	
Chapter 13	Model	ling Conta	ict		119	
	13.1	Contact	Models		119	
	13.2			odel		
		13.2.1		ment Model		
			13.2.1.1	Geometry and Mesh		
			13.2.1.2	Material Properties		
			13.2.1.3	Contact Pairs  Boundary Conditions		
		13.2.2	13.2.1.4	Boundary Conditions		
		13.2.2		1		
		13.2.4				
	13.3	2D Porc		el of Knee		
		13.3.1	Finite Elei	ment Model	131	
			13.3.1.1	Geometry and Mesh	131	
			13.3.1.2	Material Properties		
			13.3.1.3	Contact Definitions	134	
			13.3.1.4	Boundary Conditions and		
				Loading		
		1000	13.3.1.5	Solution Setting		
		13.3.2				
		13.3.3 13.3.4		1		
	Refere					
Cl 4 14	A 1'		ı D' ( I			
Chapter 14	Application of the Discrete Element Method for Study of the Knee Joint					
	14.1			rete Element Method		
	14.2			el		
		14.2.1		e Intersection		
		14.2.2		Springs		
		14.2.3	Boundary	Conditions	145	

x Contents

		14.2.4 14.2.5 14.2.6	Results	146			
	Refere		Summary				
PART IV	Sim	ulation	of Implants				
Chapter 15	Study of Contact in Ankle Replacement						
	15.1	Finite E 15.1.1 15.1.2 15.1.3 15.1.4	Clement Model	151 151 153			
	15.2						
	15.3		ion				
	15.4 Refere		ry				
Chapter 16	Simulation of Shape Memory Alloy (SMA)  Cardiovascular Stent						
	16.1	SMA M 16.1.1 16.1.2	SMA Model for Superelasticity  SMA Model with Shape Memory Effort	157			
	16.2	Simulati 16.2.1	ion of Angioplasty with Vascular Stenting Finite Element Model	. 161 162			
			16.2.1.1 Geometry and Mesh				
			16.2.1.2 Material Properties				
			16.2.1.4 Solution Setting				
		16.2.2	Results				
		16.2.3	Discussion				
	D. C	16.2.4	Summary				
	Refere	ences		. 167			
Chapter 17	Wear	Model of	Liner in Hip Replacement	. 169			
	17.1		imulation				
		17.1.1 17.1.2	Archard Wear Model				
	17.2		Improving Mesh Quality during Wear ing Wear of Liner in Hip Replacement				
	17.2	17.2.1	Finite Element Method				
			17.2.1.1 Geometry and Mach	170			

Contents xi

			17.2.1.2	Material Properties	170
			17.2.1.3	Wear Model	
			17.2.1.4	Contact Definition	
			17.2.1.5	Loading and Boundary	
			17.12.11.0	Conditions	172
			17.2.1.6	Solution Setting	
		17.2.2			
		17.2.2		n	
		17.2.3			
	D . C				
	Refere	nces	•••••		1/5
Chapter 18	Fatigue	e Analysis	s of a Mini l	Dental Implant (MDI)	177
	18.1	SMART	Crack-Gro	wth Technology	177
	18.2			fe of an MDI	
	10.2	18.2.1		ment Model	
		16.2.1			
			18.2.1.1	Geometry and Mesh	
			18.2.1.2	*	1/9
			18.2.1.3	ž ,	
				Conditions	180
			18.2.1.4	Setting up Fracture	
				Calculation	180
		18.2.2	Results		181
		18.2.3	Discussion	n	183
		18.2.4	Summary		184
	Refere	nces			184
			_		
PART V	Retro	ospecti	ive		
Chapter 19	Retros	pective			187
	19.1	Principle	es for Mode	ling Biology	187
	19.2				188
	19.3	•	•		
	19.4				
	19.5				
Appendix 1:	Input Fi	le of the I	Multidimens	ional Interpolation	
					189
Appendix 2:	Input Fi	le of the	Anisotropic	Femur Model in Section 4.2	203
Appendix 3:	Input Fi	le of the 2	XFEM Cracl	k-Growth Model in	
	Section	5.2			207

xii Contents

Appendix 4:	Input File of the Abdominal Aortic Aneurysm Model in Section 7.2	213
Appendix 5:	Input File of the Periodontal Ligament Creep Model in Section 8.2	217
Appendix 6:	Input File of the Intervertebral Disc Model with Fiber Enhancement in Section 9.1.2	221
Appendix 7:	Input File of the Intervertebral Disc Model with Mesh Independent Fiber Enhancement in Section 9.2.2	229
Appendix 8:	Input File of the Anterior Cruciate Ligament Model in Section 9.3.2.	235
Appendix 9:	Input File of Subroutine UserHyper in Section 10.2	239
Appendix 10	: Input File of the Head Impact Model in Section 11.2	243
Appendix 11	: Input File of the Intervertebral Disc Model in Section 11.3	245
Appendix 12	: Input File of the Knee Contact Model in Section 13.2	249
Appendix 13:	Input File of the 2D Axisymmetrical Poroelastic Knee Model in Section 13.3	259
Appendix 14	Input File of the Discrete Element Model of Knee Joint in Chapter 14	265
Appendix 15	Input File of the Material Definition of the Cancellous Bone in Chapter 15	273
Appendix 16	Input File of the Stent Implantation Model in Chapter 16	281
Appendix 17	Input File of the Wear Model of Hip Replacement in Chapter 17	289
Appendix 18	Input File of the Mini Dental Implant Crack-Growth Model in Chapter 18	293
Index		299

#### **Preface**

In 2001, I came to the University of Pittsburgh to pursue my PhD. As I learned about biomechanics, I became fascinated by the complications of biology. In the past 17 years, I had been working on many bioengineering projects with professors from the University of Pittsburgh, University of Pennsylvania, Allegheny General Hospital, and Soochow University. My long-time research has given me experience in finite element modeling in the field of biomedical studies. I have chosen to record my experiences in a book which, I hope, will encourage medical researchers to do further investigations. Yet, even after 17 years of study and research, I recognize that I still have more to learn about biomechanics. Should this book, therefore, contain errors, I ask readers to point them out to me so that I can address and correct them.

While I wrote this book, I received help and encouragement from many of my friends, including Frank Marx, Dr. J.S. Lin, Dr. Richard Debski, and Fayan Xu. Dr. Zhi-Hong Mao reviewed the whole manuscript. I am grateful for his constructive comments that have greatly improved the quality of the book. I give a special thanks to Ronna Edelstein for her time and effort in revising my manuscript. I express my great appreciation to the staff at CRC Press, especially Marc Gutierrez and Kari Budyk for their assistance in publishing the book. Finally, I thank my family, especially my wife, Peng, and my two children, for their constant support.



### About the Author

**Z.** Yang earned a PhD in mechanical engineering at the University of Pittsburgh in 2004. Over the last 17 years, he has collaborated with professors from various colleges, such as the University of Pennsylvania and University of Pittsburgh, and finished a number of biomedical projects. Currently, he is a senior software engineer in the field of finite element analysis with over 10 years' experience.



## 1 Introduction

Because people are living longer in today's world, more individuals are dealing with a variety of diseases. Some common diseases are associated with the mechanical states of human organs. For example, hips often break when older people fall, and the lumbar disc degenerates due to excessive loadings over the long term. An abdominal aortic aneurysm (AAA) occurs when the stresses of the AAA wall exceed the strength of the wall tissue. Treatment of these diseases requires an understanding of the stress-states of relevant parts under various conditions. When some parts of the human body degenerate and lose their function, people may have to undergo implant surgeries, such as stent implantation for treatment of atherosclerosis and total knee replacement to regain the walking function. Although these implants can improve the person's quality of life significantly, they can also raise other issues, such as medial tilting in ankle replacements and fatigue and wear of the liner in hip implants. To solve these issues and improve the medical designs, it is vital to study the mechanical behavior of the implants.

While researchers are testing the mechanical responses of the organs and the implants in the lab, they also emphasize numerical simulations, especially finite element analysis. Since the 1970s, some well-known commercial finite element codes, such as ANSYS, NASTRAN, MARC, ABAQUS, LSDYNA, and COMSOL, have been developed to solve the structural problems. Among them, ANSYS software has the most powerful nonlinear solver, and hence it has become the most widely used software in both academia and industry. Over the past decade, many advanced finite element technologies have been developed in ANSYS. The purpose of this book is to simulate some common medical problems using finite element advanced technologies, which paves a path for medical researchers to perform further studies.

The book consists of four main parts. Each part begins by presenting the structure and function of the biology, and then it introduces the corresponding ANSYS advanced features. The final discussion highlights some specific biomedical problems simulated by ANSYS advanced features.

The topic of Part I is bone. After this introductory chapter, Chapter 2 introduces the structure and material properties of bone. Chapter 3 discusses the nonhomogeneous character of bone, including modeling it by computed tomography (CT) in Section 3.1 and by multidimensional interpolation in Section 3.2. Chapter 4 describes how to build a finite element model of anisotropic bone, and the crack-growth in the microstructure of cortical bone is simulated by eXtended Finite Element Model (XFEM) in Chapter 5.

Part II, which deals with soft tissues, is very detailed. Chapter 6 introduces the structure and material properties of soft tissues like cartilage, ligament, and intervertebral discs (IVDs). Next, Chapter 7 presents the nonlinear behavior of soft tissues and simulation of AAA in ANSYS190. Chapter 8 examines the viscoelasticity of soft tissues, including its application to the study of periodontal ligament creep.

Some soft tissues are enhanced by fibers. Chapter 9 discusses three approaches of fiber enhancement in ANSYS190: (1) standard mesh-dependent fiber enhancement, in which the fibers are created within the regular base mesh; (2) mesh-independent fiber enhancement that creates fibers independent of the base mesh; and (3) the anisotropic material model with fiber enhancement. The first two approaches are utilized to simulate the fibers in the annulus of the intervertebral disc (IVD).

Many nonlinear material models in ANSYS are available for the simulation of soft tissues. If the experimental data of one biological material do not fit any of these models, the researchers may turn to USERMAT in ANSYS. Chapter 10 focuses on the topic of how to develop user material models in ANSYS.

The soft tissues are biphasic, consisting of 30%–70% water. Chapter 11 introduces ways of modeling soft tissues as porous media and the application of biphasic modeling in head impact and IVD creep research.

Part III describes joint simulation. After briefly introducing the structure of joints in Chapter 12, in the next chapter, Section 13.1 defines three contact types in a whole-knee simulation, and a two-dimensional (2D) axisymmetrical poroelastic knee model is built in Section 13.2. Then, the discrete element method of knee joint that is implemented in ANSYS is analyzed in Chapter 14.

Part IV presents a number of implant simulations. Chapter 15 studies the contact of the talar component and the bone to investigate medial tilting in ankle replacement. The stent implantation is simulated in Chapter 16 using the shape memory alloy superelasticity model. The Archard wear model is applied to study the wear of the hip implant in Chapter 17. Chapter 18 predicts the fatigue life of a mini-dental implant using ANSYS SMART technology.

Chapter 19 presents a retrospective look at the entire content of the book. Some guidelines are summarized for the simulation of biomedical problems.

The biomedical problems in this book have been simulated using ANSYS Parametric Design Language (APDL). Reading this book requires knowledge of APDL. To learn APDL, I suggest first reading the ANSYS help documentation and then practice some technical demonstration problems available in this documentation. All APDL input files of the finite element models in the book are provided in the appendixes.